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Improvement of Hyperthermia Properties of Iron Oxide Nanoparticles by Surface Coating / Vassallo, Marta; Martella, Daniele; Barrera, Gabriele; Celegato, Federica; Coisson, Marco; Ferrero, Riccardo; Olivetti, Elena S; Troia, Adriano; Sözeri, Hüseyin; Parmeggiani, Camilla; Wiersma, Diederik S; Tiberto, Paola; Manzin, Alessandra. - In: ACS OMEGA. - ISSN 2470-1343. - 8:2(2023), pp. 2143-2154. [10.1021/acsomega.2c06244]
Availability:
This version is available at: 11696/76229 since: 2023-03-01T10:35:38Z

Publisher:
AMER CHEMICAL SOC

Published
DOI:10.1021/acsomega.2c06244

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12 October 2024

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Article

Improvement of Hyperthermia Properties of Iron Oxide Nanoparticles by Surface Coating

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Cite This: *ACS Omega* 2023, 8, 2143−2154

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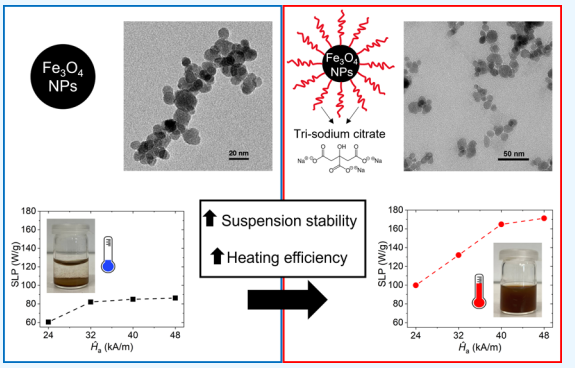
ABSTRACT: Magnetic hyperthermia is an oncological therapy that exploits magnetic nanoparticles activated by radiofrequency magnetic fields to produce a controlled temperature increase in a diseased tissue. The specific loss power (SLP) of magnetic nanoparticles or the capability to release heat can be improved using surface treatments, which can reduce agglomeration effects, thus impacting on local magnetostatic interactions. In this work, Fe_3O_4 nanoparticles are synthesized via a coprecipitation reaction and fully characterized in terms of structural, morphological, dimensional, magnetic, and hyperthermia properties (under the Hergt−Dutz limit). Different types of surface coatings are tested, comparing their impact on the heating efficacy and colloidal stability, resulting that sodium citrate leads to a doubling of the SLP with a substantial improvement in dispersion and stability in solution over time; an SLP value of around 170 W/g is obtained in this case for a 100 kHz and 48 kA/m magnetic field.



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1. INTRODUCTION

Magnetic hyperthermia is a therapy that can be used in cancer treatment, generally as an adjuvant for chemotherapy or radiotherapy. This technique is based on the use of magnetic nanoparticles (NPs), which are injected or conveyed through the circulatory system in the tumor region and then activated by an alternating current (AC) magnetic field, with the consequent release of thermal energy through hysteresis losses. The aim is to selectively increase the temperature of the tumor region from 40 to 45 °C to induce a greater response of cancer cells to drugs or radiation.[1−4] The side effects are limited as healthy cells are less thermosensitive than cancerous ones, being characterized by hypoxia and lower pH.[5,6]

Magnetic hyperthermia is a very versatile technique, which can also be used for other biomedical applications, such as drug delivery (through the controlled release of molecules encapsulated in thermolabile coatings)[4,7,8] or warming of frozen organs for transplantation.[9] Moreover, magnetic hyperthermia can be combined with photothermal therapy, using light and magnetic fields in a synergistic way to treat cancer lesions with higher efficacy.[8,10]

The magnetic nanomaterials mostly studied for hyperthermia are iron oxide NPs due to their chemical stability, easy surface coating, and high biocompatibility in terms of safety and body clearance.[2,8,11] The biocompatibility and biosafety of iron oxide NPs have been assessed by numerous cytotoxicity studies performed on different cell lines.[12] Some formulations based on iron oxide NPs have also been approved by the Food and Drug Administration (FDA) and the European Medicines Agency (EMA) for therapeutic and diagnostic applications, such as the treatment of iron deficiency, magnetic resonance imaging (MRI), and cancer therapy[4,11,13]. In particular, clinical studies of magnetic hyperthermia have been already conducted on prostatic carcinoma and glioblastoma multiforme using NanoTherm ferrofluid, consisting of iron oxide NPs covered with aminosilane.[14−16]

The capability of magnetic NPs to release heat is generally expressed through the specific loss power (SLP), which is the power dissipated per unit mass of magnetic material.[17] Material properties, size, shape, and state of aggregation are the main parameters that can influence the SLP.[18−23] Regarding material properties, precise tuning of magnetocrystalline anisotropy and applied magnetic field parameters can lead to an increase in the heating efficiency, as documented for cobalt and zinc ferrite NPs.[24−27] Size should be accurately modified to obtain an optimum heating efficiency, as demonstrated by cubic iron oxide NPs, which show a maximum SLP around 100 nm.[28] Shape has

Received: September 27, 2022
Accepted: December 15, 2022
Published: January 4, 2023

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also a key role; very high SLP values have been reported for flower-, disk-, ring-, and octahedron-like NPs, which, however, require for their synthesis controlled pressures and high temperatures[29−32] or nanolithography techniques[33] that are difficult to be scaled up at industrial level.

Regarding the state of aggregation, the formation of NP clusters or chains driven by magnetostatic dipole−dipole interactions can be responsible for a significant variation in the SLP,[34,35] e.g., the arrangement in chains typically results in larger SLP values,[28] while large clusters usually lead to worse heating performance. However, the collective magnetic behavior due to interparticle interactions can be beneficial to hyperthermia for small aggregates, whose optimal size depends on the material composition.[26,36]

One of the best strategies to minimize detrimental magnetostatic interactions is to functionalize the surface of the NPs with organic or inorganic coatings, which favor their dispersion via the formation of a steric hindrance and/or a surface charge that triggers repulsive electrostatic interactions.[37−39] The coatings not only increase the colloidal stability but can also improve the biocompatibility of NPs, allowing their suspension in aqueous or organic media and enabling the binding with other functional groups or molecules useful for addressing specific functions in therapeutics and diagnostics.[5,38]

In this paper, we focus on the chemical synthesis, via a coprecipitation method, of Fe_3O_4 NPs and on the functionalization of their surface with nontoxic coating agents based on sodium citrate or carboxymethyl cellulose (CMC), investigated to improve the heating efficiency and colloidal stability of bare NPs. Sodium citrate was chosen for its high biocompatibility, as documented by its large use in the food and pharmaceutical industry.[40] Citrate ions have indeed a strong coordination affinity with iron ones, thus favoring NP chemisorption;[41,42] moreover, the carboxylate groups can promote the processes of cellular transport and internalization of NPs.[12,43] CMC, a water-soluble polymer derived from cellulose by hydroxyl group substitution with carboxymethyl groups, was chosen because it can increase blood circulation time. Moreover, the carboxylic groups, not directly bonded on the NP surface, can be used for further functionalization with other molecules, e.g., for targeting in drug delivery.[44−46]

The prepared NPs were first characterized in terms of structural, morphological, and dimensional properties by means of X-ray diffractometry (XRD) and transmission electron microscopy (TEM) imaging. The effective presence of surface coating was analyzed via Fourier transform infrared (FTIR) spectroscopy and thermogravimetric analysis (TGA), followed by the investigation of colloidal stability and hydrodynamic size through dynamic light scattering (DLS) characterization. Magnetic properties were studied in detail, measuring both the static hysteresis loops of dry samples and the dynamic hysteresis loops of liquid samples. The latter results were correlated with the outputs from thermometric characterization, performed under a 100 kHz magnetic field with an amplitude of up to 48 kA/m. In this way, we guaranteed the fulfillment of the Hergt−Dutz limit, that is, $\hat{H}_a f \leq 5 \times 10^9$ A/(m s),[47,48] where $\hat{H}_a$ and f are the peak amplitude and frequency of the applied AC magnetic field, respectively. Above this limit, non-negligible eddy current effects associated with the heating of healthy tissues were previously observed in preclinical tests conducted on mice and rats[49] as well as predicted by *in silico* models.[50] The SLP values estimated from thermometric characterization were finally corroborated by thermal simulations performed with an in-house heat transfer solver.[51]

2. EXPERIMENTAL SECTION

2.1. Materials. All materials employed for sample preparation, i.e., iron(II) chloride tetrahydrate ($FeCl_2{\cdot}4H_2O$), iron(III) chloride hexahydrate ($FeCl_3{\cdot}6H_2O$), ammonium hydroxide solution (NH_4OH, 30%), sodium carboxymethyl cellulose (average molecular mass of ∼90 kDa), and tri-sodium citrate dihydrate ($C_6H_5Na_3O_7{\cdot}2H_2O$) were purchased from Sigma-Aldrich and used without further purification.

2.2. Synthesis and Surface Coating. Fe_3O_4 NPs were synthesized through the coprecipitation method.[52] Briefly, iron(II) chloride tetrahydrate and iron(III) chloride hexahydrate were dissolved in deionized water with a molar ratio of Fe^{2+}/Fe^{3+} equal to 1:2 and an iron concentration of 0.5 M. The reaction was carried out in a total volume of 100 mL of water under vigorous stirring and nitrogen flow for its entire duration. Following the complete dissolution, the mixture was heated up to 75 °C and precipitation was achieved by adding a 15 mL solution of ammonium hydroxide (30%) dropwise to reach the pH of 8.0−8.5. The precipitate was heated up to 85 °C for 1 h, washed with deionized water until reaching neutral pH, and magnetically decanted to separate the synthesized Fe_3O_4 NPs.

For the citrate coating, dried Fe_3O_4 NPs were suspended in 50 mL of water (2% w/v) and sonicated for 10 min. An aqueous solution of 4% w/v tri-sodium citrate dihydrate was prepared under stirring and added to the above suspension with a molar ratio of 6.4 (Fe_3O_4/citrate). The obtained mixture was sonicated in a sonicator bath and heated up to 60 °C for 1 h. The material was washed three times with deionized water and recovered by magnetic separation.

For the CMC coating, dried Fe_3O_4 NPs were suspended in 15 mL of water (1% w/v) and sonicated for 10 min. An aqueous solution of 0.1% w/v CMC (10 mL) was obtained under stirring and added dropwise to the magnetic suspension. The mixture was stirred overnight, and the Fe_3O_4 NPs were collected magnetically and washed three times with deionized water.

2.3. Structural, Morphological, and Dimensional Characterization. The crystal phase of the Fe_3O_4 NPs was analyzed by X-ray diffractometry (XRD), using a Panalytical X'Pert PRO MPD diffractometer with Cu Kα radiation (λ = 1.541874 Å) in the 2θ; range from 8 to 100°. The obtained XRD pattern was investigated considering the square root of the intensities to highlight low intensity reflection signals and compared with the XRD data for Fe_3O_4 (ICDD PDF card no. 01-075-0033).

Morphology and size distribution of the Fe_3O_4 NPs were determined by means of transmission electron microscopy (TEM), employing a JEOL JEM-2100 transmission electron microscope. Transmission electron microscopy (TEM) images were analyzed by the open-source software ImageJ;[53] the mean size was estimated by performing statistical analysis on 160 NPs.

2.4. Characterization of Surface Coating and Colloidal Stability. The presence of a coating bounded to the surface of the Fe_3O_4 NPs was investigated by Fourier transform infrared (FTIR) spectroscopy using a Shimadzu FTIR spectrometer, model IRAffinity-1S.

The composition of the Fe_3O_4 NPs was determined by thermogravimetric analysis (TGA), employing a TA Instruments Discovery SDT 650 analyzer, operating with a temperature ramp up to 1000 °C and applying a constant heating rate of

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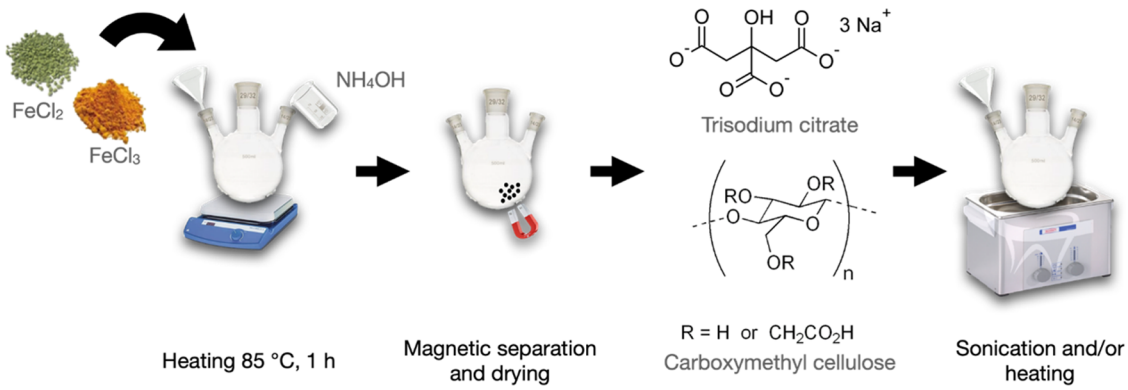

Figure 1. Schematic representation of the chemical preparation via coprecipitation of Fe_3O_4 NPs and their coating with tri-sodium citrate or CMC.

10 °C/min. TGA results enabled the evaluation of the amount of coating bounded to the surface of the NPs.

The colloidal stability and hydrodynamic size of the Fe_3O_4 NPs were investigated by dynamic light scattering (DLS) using a Beckman Coulter DelsaNano ζ potential and submicron particle size analyzer. DLS results were obtained with at least three scans for each measurement.

The above instrument was also used to evaluate the surface charge of the Fe_3O_4 NPs by ζ potential measurements conducted on the magnetic suspensions at neutral pH. ζ potential results were obtained with at least three scans for each measurement.

Colloidal stability was also monitored in time by observing the NP suspensions after 6 months, following their preparation, and by characterizing the NPs encapsulated in hydrogels. For the encapsulation, agarose was added to an aqueous suspension of Fe_3O_4 NPs, with a concentration of 5 mg/mL, to obtain a concentration of 1% w/v. The mixture was then heated at 80 °C for 10 min to dissolve the agarose and cooled down to form the gel.

2.5. Magnetic Characterization. The static hysteresis loops of dry samples were measured at room temperature by vibrating sample magnetometry (VSM), employing a Lake Shore 7410 magnetometer. The characterization was performed under direct current (DC) magnetic fields, varying from −1352 to 1352 kA/m in steps of 0.8 kA/m.

Dynamic hysteresis loops were measured at room temperature by a custom-built B−H tracer[54] under the application of a uniform AC magnetic field with a frequency of 69 kHz and an amplitude selectable up to 36 kA/m. The measurements were performed on samples made of an aqueous suspension of uncoated or coated Fe_3O_4 NPs with a concentration of 10 and 12 mg/mL, respectively.

2.6. Thermometric Characterization. Thermometric measurements were performed with a custom-built setup.[55] The aqueous suspensions of uncoated or coated Fe_3O_4 NPs, with a concentration of about 12 mg/mL, were poured into a test tube and then exposed to a uniform AC magnetic field with a frequency of 100 kHz and an amplitude selectable in the range 24−48 kA/m, thus fulfilling the Hergt−Dutz limit.[47,48] The heating time was fixed to 1 h for each measurement. A fiber optic thermometer (Osensa Innovation), with the sensing point placed at the suspension center, was used to measure the local temperature during the heating and cooling transients. Then, the recorded curves of the temperature time evolution were processed using a fitting function derived from an analytical thermodynamic model,[55] allowing the estimation of the specific loss power (SLP) of NPs.

2.7. Heat Transfer Modeling. The thermometric characterization was supported by thermal simulations carried out with an in-house 3D finite element code, which solves the heat transfer equation under the assumption of negligible convection phenomena.[28,51] This results in

$$\rho C_p \frac{\partial T}{\partial t} = \nabla \cdot k \nabla T + Q_{ext} + \frac{\mathrm{SLP} \cdot m_{NPs}}{V_{water}} \quad (1)$$

where T is the temperature, ρ is the mass density, C_p is the heat capacity, and k is the thermal conductivity. SLP is the NP specific loss power estimated from the thermometric characterization, m_{NPs} is the mass of magnetic NPs within the particle-fluid suspension, where the NPs are assumed to be uniformly dispersed and V_{water} is the water volume. Q_{ext} is the heating power per unit volume due to the AC magnetic field source; this includes parasitic eddy current heating effects and is derived from preliminary thermometric measurements performed on a sample of water with volume V_{water}.

Equation 1 is completed by the following boundary condition

$$k \nabla T \cdot \boldsymbol{n} = h(T_{ext} - T) \quad (2)$$

where $\boldsymbol{n}$ is the outward normal vector to the boundary surface, h is the heat transfer coefficient, which considers convective cooling effects, and T_{ext} is the time-dependent external temperature. At $t = 0$, $T = T_{ext}$ in all of the domains of analysis.

3. RESULTS AND DISCUSSION

3.1. Preparation and Surface Coating of Fe_3O_4 Nanoparticles. A schematic of the Fe_3O_4 NP synthesis and coating is reported in Figure 1. The synthesis was performed with a simple and large-scale process that involves coprecipitation in an alkaline environment. Starting from a mixture containing Fe^{2+} and Fe^{3+}, the NPs were precipitated with ammonium hydroxide solution and heated up to 85 °C. After magnetic recovery and washing with water, a large quantity of NPs was obtained, corresponding to a yield of 72.7% (mass of 1.7 g). The reproducibility of the coprecipitation method was verified by synthesizing the second batch of Fe_3O_4 NPs using the same synthesis conditions described above. To test the reproducibility in terms of heating properties, we performed also on this sample magnetic and thermometric characterizations (as described in the following subsections).

Moreover, surface coating processes were performed to modify the colloidal stability of the NPs and thus improve their hyperthermia properties. A solution of the coating agent (tri-

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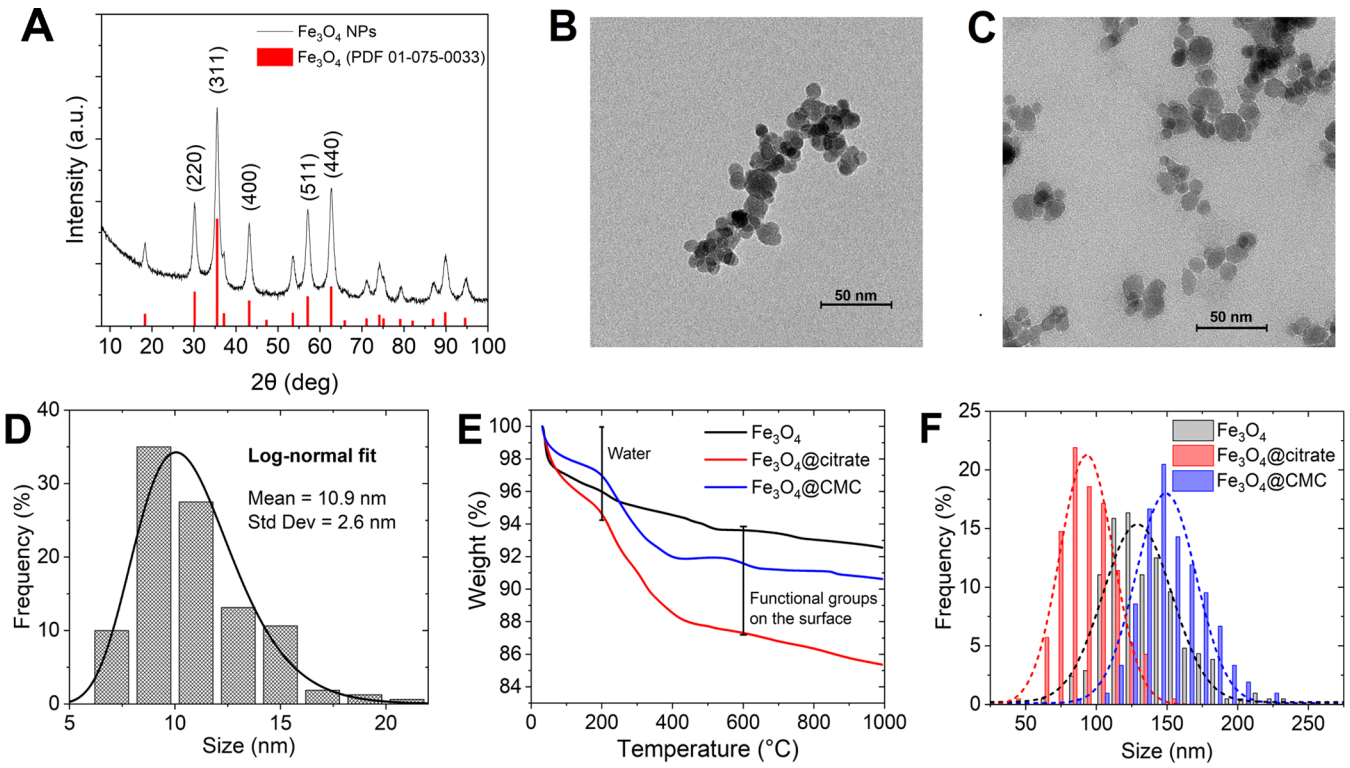

Figure 2. (A) XRD pattern of the uncoated Fe_3O_4 NPs, reporting the square root of the intensities; the characteristic diffraction peaks of Fe_3O_4 (ICDD PDF card no. 01-075-0033) are indicated with the red vertical lines for comparison. Representative TEM images of (B) uncoated and (C) citrate-coated NPs. (D) Size distribution histogram (derived from statistical analysis on TEM images of uncoated NPs). (E) TGA curves and (F) DLS particle size distribution for uncoated (black), citrate-coated (red), and CMC-coated (blue) NPs (the reported Gaussian fits are a guide to the eye).

sodium citrate or CMC) was added to a Fe_3O_4 NP suspension and subjected to heating and/or sonication. The NPs were purified another time by magnetic decantation, followed by washing with water.

3.2. Analysis of Crystal Phase, Dimension, Surface Coating, and Colloidal Stability. Dried Fe_3O_4 NPs were first characterized in terms of crystal structure, size, and shape. The XRD pattern for uncoated NPs is shown in Figure 2A, revealing a crystalline phase with main diffraction peaks indexed as (220), (311), (400), (511), and (440), such as for the cubic spinel structure of Fe_3O_4 (ICDD PDF card no. 01-075-0033). The comparison to the XRD pattern of Fe_2O_3 (ICDD PDF card no. 00-039-1346), as reported in Figure S1, enables us to confirm the Fe_3O_4 composition of the uncoated NPs and to exclude the presence of Fe_2O_3 phase, as its characteristic extra peaks (around 15, 24, and 26°) are not observable.[56,57]

Representative TEM images of uncoated and citrate-coated Fe_3O_4 NPs are reported in Figure 2B,C, respectively (the corresponding image for CMC-coated Fe_3O_4 NPs is shown in Figure S2). The NPs have a quasi-spherical shape and are strongly uniform in size, exhibiting a narrow size distribution well fitted by a log-normal distribution function with a mean value of 10.9 nm and a standard deviation of 2.6 nm. This is well demonstrated by the histogram in Figure 2D, derived from statistical analysis of TEM images performed on the Fe_3O_4 NPs by means of ImageJ software.[53] From TEM images, it is also possible to observe differences in the aggregation state of the samples. The uncoated Fe_3O_4 NPs are arranged in aggregates with dimensions around 130 nm (Figure 2B) as a possible consequence of strong magnetic dipole−dipole interactions. Similar aggregates are observed for the CMC-coated Fe_3O_4 NPs (Figure S2), while those with the citrate-based coating are clustered in smaller aggregates (Figure 2C).

The presence of surface coating, based on tri-sodium citrate or CMC, was confirmed by different characterization techniques, comprising FTIR spectroscopy, TGA, and DLS analysis. The FTIR spectra of uncoated and coated Fe_3O_4 NPs are shown in Figure S3. For the uncoated NPs, the measured spectra are characteristic of Fe_3O_4 NPs, where the band at 580−630 cm^{-1} corresponds to the vibration of the Fe−O bond, while the peaks at 1624 and 3400 cm^{-1} can be attributed to the bending and stretching vibrations of the hydroxyl groups of the water molecules adsorbed on the sample surface.[45] In the spectra of the citrate- and CMC-coated NPs, two and three new peaks appear at 1381, 1616 cm^{-1} and 1059, 1417, 1623 cm^{-1}, respectively. The peaks at 1381 and 1616 cm^{-1} can be attributable to the symmetric and asymmetric stretching vibration of COO^- groups of citrate anions, respectively.[58,59] The peaks at 1059, 1417, and 1623 cm^{-1} correspond, in the order, to the stretching vibration of the O−C−C bond and the symmetric and asymmetric stretching vibration of the −COO bond in the structure of carboxylic salt. The presence of new peaks demonstrates that the coating agents were effectively bonded to the surface of the Fe_3O_4 NPs.[44,45,60]

The thermographs of uncoated and coated Fe_3O_4 NPs, obtained with TGA, are shown in Figure 2E. The initial weight loss at temperatures below 200 °C refers to the desorption of water molecules. The thermogravimetric curve of the uncoated NPs shows that the weight loss in this range is about 4%, while that of the coated NPs reports a weight loss of 5.4 and 3% for citrate- and CMC-coated Fe_3O_4 NPs, respectively; these small variations are simply due to the different content of water molecules in the samples. The following weight loss for

https://doi.org/10.1021/acsomega.2c06244
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temperatures between 200 and 1000 °C is due to the decomposition of the coating agent adsorbed on the surface of the NPs. This is in the order of 9.2 and 6.4% for citrate- and CMC-coated NPs, respectively; the observed weight loss indicates that a greater quantity of coating agent is adsorbed on the surface of the NPs treated with citrate rather than with CMC.

Finally, we analyzed the stability of NPs in solution, an important parameter for their potential biomedical applications. The hydrodynamic size distributions characterized by DLS are shown in Figure 2F, and the mean hydrodynamic size, the relative polydispersity index, and the ζ potential value of each sample are reported in Table 1. DLS and ζ potential measurements were performed on both uncoated and coated NPs to investigate possible changes in sample dispersion resulting from the surface coating process. Through DLS, it is possible to characterize the hydrodynamic behavior of NPs or, more precisely, the size of the aggregates in which they are organized; however, this technique does not allow us to discriminate between the inorganic material and the organic material of the coating. The mean hydrodynamic size for the uncoated NPs was around 135 nm, confirming the size of the aggregates observed in TEM images (Figure 2B). The improvement in the dispersion of the citrate-coated Fe_3O_4 NPs, caused by a decrease in the aggregate size already documented by the TEM image in Figure 2C, was also demonstrated by the smaller value of the mean hydrodynamic size, which was in the order of 95 nm. Conversely, the CMC-coated NPs are organized in aggregates with larger dimensions than the ones of uncoated NPs, with sizes in the order of 150 nm. Thus, the introduction of surface coating leads to a variation in the aggregate size, which strongly depends on the coating type, as already demonstrated in the literature via DLS measurements.[61]

Table 1. Mean Hydrodynamic Size (Derived from Gaussian Fit), Polydispersity Index (PDI) and ζ Potential Values Obtained for the Three Samples (Uncoated, Citrate-Coated, and CMC-Coated NPs)

sample	mean hydrodynamic size (nm)	PDI	ζ potential (mV)
Fe_3O_4	135 ± 35	0.277	−24.8 ± 0.5
Fe_3O_4@citrate	95 ± 18	0.251	−26.1 ± 1.4
Fe_3O_4@CMC	152 ± 27	0.276	−26.8 ± 1.0

The polydispersity index values are comparable between the samples, and this demonstrated that the width of the size distribution is similar, although the hydrodynamic size of the NP aggregates changes because of the surface treatment.

The ζ potential measurements provide information on the surface charge of NPs, and it is known that for absolute values greater than 30 mV, the suspension is characterized by good colloidal stability and a low tendency to flocculate.[62] The ζ potential for the uncoated NPs, measured at neutral pH, was −24.8 ± 0.5 mV, in agreement with the values registered for Fe_3O_4 NPs.[63] ζ potentials of −26.1 ± 1.4 and −26.8 ± 1.0 mV were obtained for the citrate- and CMC-coated NPs.

The above increase in the absolute value of the ζ potential, although modest, demonstrated the adsorption of negatively charged carboxylic groups on the NP surface.[44,58] The slight increase in ζ potential can be attributable to the small amount of coating agents on the surface of Fe_3O_4 NPs, as can also be seen from the TGA results.

3.3. Analysis of Static and Dynamic Magnetic Properties. The room-temperature $M(H)$ curves of uncoated, citrate-coated, and CMC-coated Fe_3O_4 NPs are shown in Figure 3. The measured magnetic signal was normalized to the Fe_3O_4 mass contained in each sample, after having appropriately subtracted that of the coating using the results from TGA (see Figure 2E). The major hysteresis loops of the three samples practically overlap since the different coatings do not affect the magnetic behavior of the samples in dry form under static conditions. The hysteresis loop of the additionally prepared uncoated Fe_3O_4 NPs is reported in Figure S4A, showing practically no differences with respect to the results in Figure 3, as proof of the reproducibility of the preparation method.

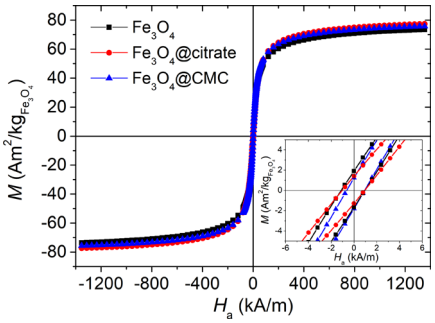

Figure 3. Room-temperature $M(H)$ curves of uncoated and coated Fe_3O_4 NPs in dry form. The magnetization values are normalized to the Fe_3O_4 mass, subtracting the coating mass obtained from TGA results. A hysteretic behavior can be inferred from the inset, which shows the portion of the hysteresis loops zoomed around coercivity.

The saturation magnetization (M_S) was determined by fitting the large field portion of the hysteresis loops with the well-known expression[64]

$$M = M_S\left(1 - \frac{\delta}{H_a} - \frac{\gamma}{H_a^2}\right) + \chi H_a \quad (3)$$

where parameters δ and γ were set as free, while χ was fixed to zero, since for the considered samples, its effect was estimated to be negligible due to the absence of paramagnetic features.

From eq 3, M_S results to be around 76 Am^2/kg; its lower value, compared to that of bulk magnetite (92 Am^2/kg),[65] can be ascribed to effects of canting or disorder of the magnetic spins at the surface of the Fe_3O_4 NPs.[66,67] For all samples, the magnetization reversal follows a sigmoidal trend with a very slow approach to saturation, which is not fully reached even at the maximum applied field. In addition, a hysteretic behavior is observable at low applied magnetic fields, resulting in a small coercivity H_c of about 1 kA/m (inset of Figure 3). Such features suggest that the samples mainly consist of interacting superparamagnetic NPs.

The above hypothesis is corroborated by TEM and DLS results (Section 3.2). On the one side, the TEM size distribution (see Figure 2D) indicates that the NPs are characterized by an average diameter (∼10 nm) mainly below the critical value (d_c) at which the transition from superparamagnetism to ferromagnetism is expected to occur. In particular, d_c is estimated in the range of 17−21 nm, when considering the common values of effective anisotropy for Fe_3O_4 ($(2-4) \times 10^4$ J/m^3).[68−70] Only a small tail of the size distribution exceeds the evaluated d_c values.

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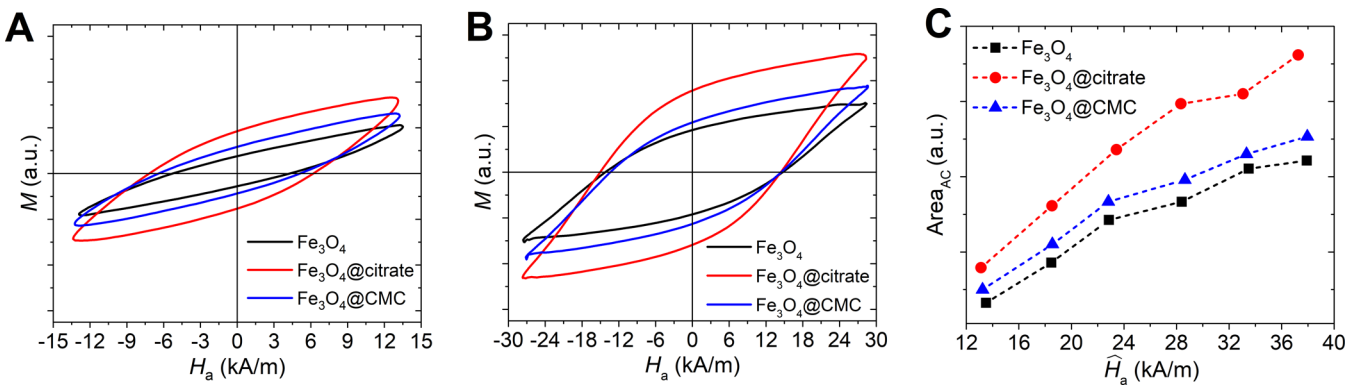

Figure 4. Dynamic minor hysteresis loops for uncoated (black), citrate-coated (red), and CMC-coated (blue) Fe_3O_4 NPs for a magnetic field with peak amplitude $\hat{H}_a$ of (A) 13.3 kA/m and (B) 28.4 kA/m. All of the hysteresis curves are normalized to the sample mass and reported in arbitrary units with the same inferior and superior limits to enable direct comparison. (C) Areas of the dynamic hysteresis loops versus $\hat{H}_a$, evaluated for all of the considered samples. All measurements were performed with a frequency of 69 kHz.

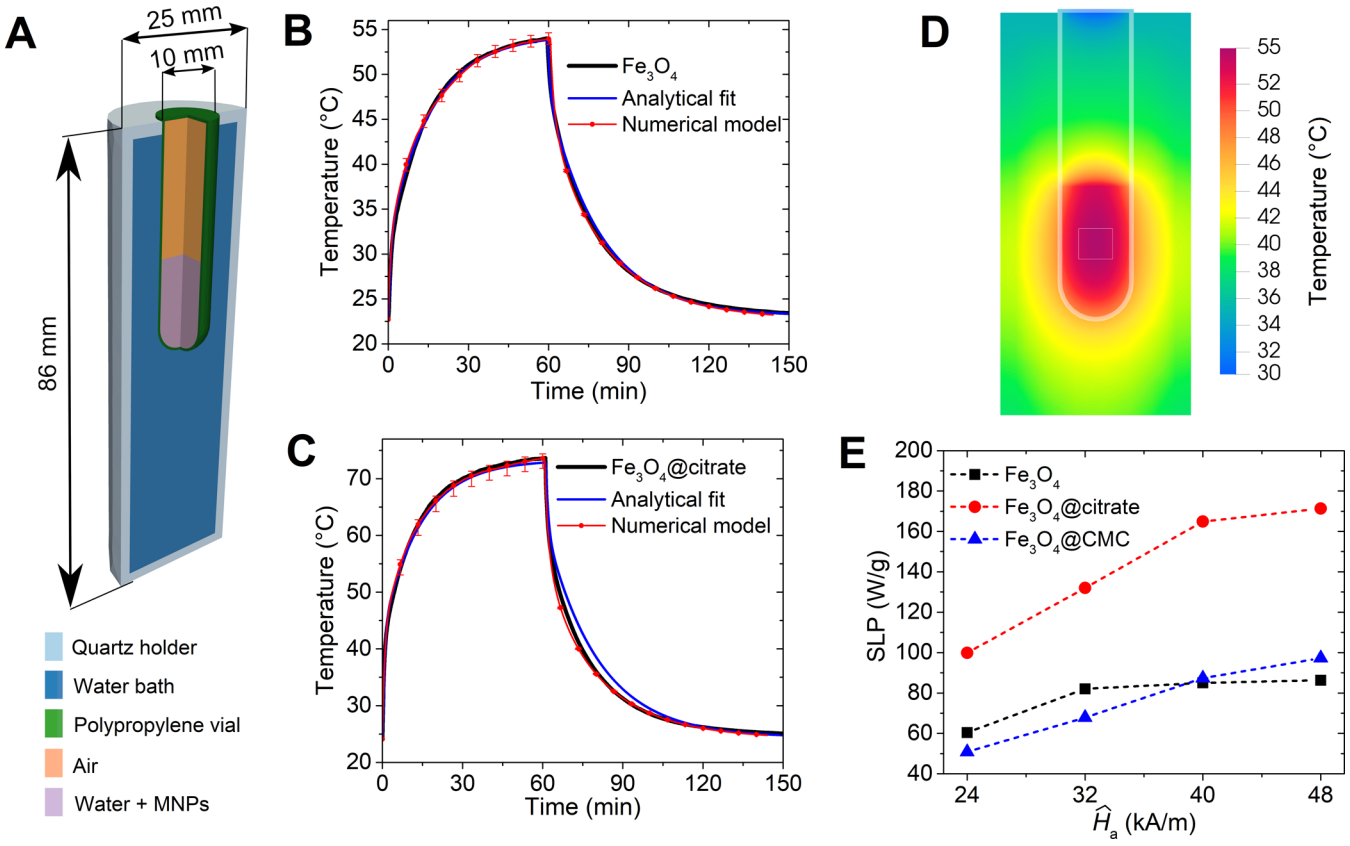

Figure 5. (A) Schematic of the sample container, corresponding to the domain considered for the heat-transfer numerical modeling. Time evolutions of the temperature of the magnetic suspensions containing (B) the uncoated NPs and (C) the citrate-coated NPs, following the application for 60 min of an AC magnetic field with a peak amplitude of 48 kA/m and a frequency of 100 kHz. The graphs contain the experimental data, the best fit outputs of the analytical thermodynamic model and the results obtained with the heat-transfer numerical model. (D) Spatial distribution of the temperature, calculated for the uncoated NP sample at the end of the heating interval. (E) SLP values for uncoated and coated NPs obtained at different peak amplitudes of the AC magnetic field, fixing the frequency to 100 kHz.

Consequently, for practically, all the single NPs, a superparamagnetic regime should be expected, in which the $M(H)$ curve follows the nonhysteretic Langevin function (i.e., zero coercivity and zero remanence). On the other hand, the NP arrangement in aggregates, as revealed by the TEM images (Figure 2B,C) and DLS size distribution (Figure 2F), leads to the formation of magnetic structures (with an effective diameter larger than d_c), in which the magnetic moments respond coherently to the applied magnetic field, thus inducing the small hysteresis observed under static conditions.[71]

AC magnetometry was then performed to investigate the capability of the NPs to release heat when exposed to AC magnetic fields with frequency f and peak amplitude $\hat{H}_a$, satisfying the Hergt−Dutz limit.[47,48] In particular, the dynamic hysteresis loops of aqueous suspensions containing both uncoated and coated Fe_3O_4 NPs were measured by applying an AC magnetic field with $f = 69$ kHz and $\hat{H}_a$ limited to 36 kA/m.

https://doi.org/10.1021/acsomega.2c06244
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Table 2. Comparison of the Results from Our Study to Data from the Literature Regarding the Heating Efficiency of Spherical Fe_3O_4 NPs

refs	size (nm)	coating	coating procedure	$\hat{H}_a$(kA/m)	f (kHz)	SLP	ILP (nHm^2/kg)
our study	10			24	100	60.4	1.05
		citrate	post			99.8	1.73
		CMC				50.8	0.88
				48		86.3	0.37
		citrate	post			171	0.74
		CMC				97	0.42
76	13			15.9	252	63.4	0.99
		citric acid	post			65.8	1.03
		APTES				67.2	1.05
		dextran				55.6	0.87
77	8.5			24	418	125	0.52
		oleic acid	post			60	0.25
		citrate				120	0.50
78	21.8			26.6	265	80	0.43
	15.1	chitosan	post			118.8	0.63
79	20			26.6	265	38.4	0.20
	5	oleic acid	post			33.5	0.18
	10	PEG				28.3	0.15
80	21			23.9	765	440	1.01
	8	citrate	*in situ*			190	0.44
	20	CTAB				95	0.22
	22	dextran				360	0.83
81	12.5			13.5	333	100	1.65
	5.9	dextran	*in situ*			36	0.59
	11	polyvinylpyrrolidone (PVP)				160	2.64
	9.5	PEG				70	1.15
	5	poly(acrylic acid) (PAA)				2	0.03
	7.5	hyaluronic acid (HA)				40	0.65
82	8			23.5	312	39.5	0.23
	9.3	oleic acid 0.2%	*in situ*			34.81	0.20
	8.3	oleic acid 0.5%				23.36	0.14
	10	oleic acid 1.0%				45.98	0.21
83	10.2			14.7	276	30	0.50
	11.7	fucoidan	post			156	2.62
	6.4	fucoidan	*in situ*			100	1.68

The hysteresis curves for $\hat{H}_a$ equal to 13.3 and 28.4 kA/m are reported in Figure 4A,B, respectively, while the entire set of AC magnetometry results is provided in Figure S5. The vertical axis is reported in arbitrary units since the output signal from the custom-built B−H tracer is not related to the magnetization value by a proper calibration procedure. However, all hysteresis curves are normalized to the sample mass to enable the comparison of the magnetic properties of the studied samples.

For all of the analyzed cases, the two branches of the hysteresis loops overlap only when the applied magnetic field reaches $\hat{H}_a$, thus leading to minor loops. Consequently, the coercivity H_c of such loops is a function of $\hat{H}_a$. However, the values of H_c result higher than the ones of the corresponding static major hysteresis loops (inset of Figure 3) due to the relaxation effects associated with the dynamic response to the AC excitation. These effects are responsible for the appearance of a well-defined hysteretic behavior, characterized by loops with a non-negligible area and thus leading to an effective release of energy, which can be exploited for magnetic hyperthermia.[72]

The areas of the dynamic hysteresis loops as a function of $\hat{H}_a$ are shown in Figure 4C for all of the studied samples. The sample containing the citrate-coated Fe_3O_4 NPs (red curve) is characterized by a larger loop area (i.e., higher heating efficiency) than the other two samples over the entire range of values considered for $\hat{H}_a$. Conversely, the CMC-based coating (blue curve) leads to a small increase in the loop area values, in comparison with the uncoated NPs (black curve). These results may be related to the ability of the citrate-based coating to reduce the size of the NP aggregates, thus improving dispersion properties, as shown in Figure 2F.

3.4. Quantitative Analysis of Heating Efficiency. In addition to AC magnetometry, thermometric measurements were performed to obtain a quantitative estimation of the coating effect on the heating efficiency of the studied NPs. The characterization was performed on liquid suspensions within a polypropylene test tube immersed in a water bath contained in a quartz holder (see the schematic in Figure 5A). As an example, Figure 5B,C illustrates the heating−cooling transients for aqueous solutions with the uncoated and citrate-coated Fe_3O_4 NPs, respectively. The thermal curves were obtained after exposing the NPs for 60 min to an AC magnetic field with a peak amplitude of 48 kA/m and a frequency of 100 kHz, thus satisfying the Hergt−Dutz limit.[47,48] The used concentration of NPs was 12 mg/mL to ensure the maintenance of good stability of the magnetic solution and temperature values in a suitable range during the measurements.

https://doi.org/10.1021/acsomega.2c06244
ACS Omega 2023, 8, 2143−2154

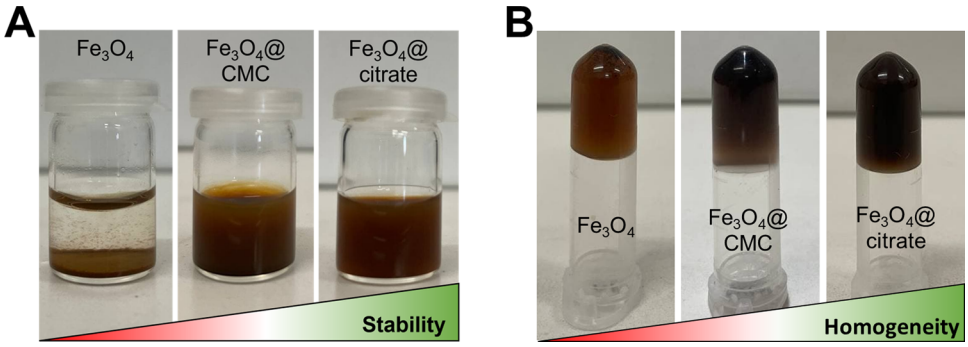

Figure 6. (A) Images of magnetic solutions, taken after 6 months from their synthesis. (B) Images of agarose gels with encapsulated NPs. The comparison was made between uncoated, citrate-coated, and CMC-coated NPs.

An analytical thermodynamic model,[55] considering the multiple heat-exchange mechanisms occurring in the experimental setup, was used to fit the experimental curves and estimate the specific loss power (SLP) of NPs as a measure of their heating efficiency. The obtained results were corroborated by the simulations carried out with the heat-transfer finite element solver described in Section 2.7, allowing us to determine the spatial distribution of the temperature within the magnetic suspension during the heating−cooling transients. The numerical simulations were performed under nonadiabatic conditions on the system schematized in Figure 5A, considering the following material properties:

- polypropylene test tube: ρ = 2600 kg/m^3; C_p = 820 J/(kg K); k = 3 W/(m K);
- quartz holder: ρ = 905 kg/m^3; C_p = 1900 J/(kg K); k = 0.185 W/(m K);
- magnetic suspension: ρ = 1020 kg/m^3; C_p = 4086 J/(kg K); k = 0.61 W/(m K).

The coefficient of convective exchange h between the holder surface and the surrounding air was set at 14 W/(m^2 K). The heating power Q_{ext} produced by the AC magnetic field sources was estimated to be 45 kW/m^3 from preliminary thermometric measurements on only water.

The fitting analytical curves and the numerical results are reported in Figure 5B,C, demonstrating a good reconstruction of the experimental data for both the uncoated and citrate-coated NP suspensions. In particular, the numerical curves were calculated in correspondence with the magnetic suspension center, where the sensing point of the fiber optic thermometer is expected to be placed. The uncertainty bars refer to the temperature variations within a volume around the suspension center, as depicted in Figure 5D, which shows the temperature map at the end of the heating phase for the sample containing the uncoated NPs.

The SLP values, derived from the experimental data fitting and validated via numerical modeling, are reported in Figure 5E and Table S1 as a function of $\hat{H}_a$ for all of the considered samples. The SLP values of the additionally prepared uncoated Fe_3O_4 NPs are reported in Figure S4B, showing negligible differences with respect to the results in Figure 5E, as an ulterior proof of the reproducibility of the preparation method.

In accordance with the outcomes of the dynamic hysteresis loop measurements (see Figure 4), the citrate-coated NPs are the most thermally efficient ones in the whole considered range of $\hat{H}_a$, showing an SLP close to 170 W/g when $\hat{H}_a$ = 48 kA/m (50% larger than the one of uncoated NPs). Conversely, the CMC-coated NPs do not lead to a substantial improvement in heating efficiency. When $\hat{H}_a$ = 48 kA/m, they approach 100 W/g with an increasing trend, while the uncoated NPs show an SLP in the order of 85 W/g, already reached at 32 kA/m.

These results on the heating efficiency are mainly related to the Neél relaxation mechanism, although the thermometric measurements were performed on NPs dispersed in a liquid, the Brown relaxation mechanism is indeed hindered by the large hydrodynamic volume of the NP aggregates (Figure 2F). In particular, the Brown relaxation time roughly estimated for each sample is orders of magnitude longer than the relaxation time $\tau = 1/(2\pi f)$ related to the used operating frequency, thus resulting in a negligible effect.[73] The heating contribution from the Neél relaxation mechanism is influenced by the effective volume of the magnetic structures that coherently respond to the AC magnetic field. The variations in the SLP values between the citrate-coated NPs and the other two samples can be attributable to the different sizes of the NP aggregates (95 nm against 130 and 150 nm for the uncoated and CMC-coated NPs, respectively). A simple model proved that the heating efficiency in samples containing clusters of NPs with a diameter lower than 15 nm decreases as the size of the aggregate increases (i.e., if the number of NPs in the aggregate increases).[74]

In summary, the 50% increase in the SLP achieved with the citrate-based surface treatment after preparation is a very promising result, also in comparison with the data available in the literature for spherical Fe_3O_4 NPs, summarized in Table 2. This table also reports the values of the intrinsic loss power (ILP), which is defined as the SLP normalized to $\hat{H}_a^2$ and f, assuming as a first approximation a linear dependence of SLP on ($\hat{H}_a^2 \cdot f$). However, this dependence is not appropriate for all of the applied field amplitudes and frequencies, resulting in an ILP that can be considered constant only in relatively low field amplitude and frequency regimes.[17,48,75] This is the reason why the ILP values of both the uncoated and coated Fe_3O_4 NPs here synthesized are not constant for the values of $\hat{H}_a$ we used in thermometric characterization (within the range 24−48 kA/m). Anyway, the ILP found for the citrate-coated NPs (0.74−1.73) results to be quite large for all of the considered magnetic field peak amplitudes, as also proved by the comparison with the other data in the literature.

In previous works, the postsynthesis coating with citrate, typically adopted for improving colloidal stability, does not lead to a significant improvement of hyperthermia properties with respect to the uncoated NPs.[76,77] Conversely, the use of chitosan allowed to obtain an increase in the SLP of around 48%, but this data was found under conditions that exceed the Hergt−Dutz limit.[78] The postsynthesis coating can also be responsible for a detriment of the NP heating efficiency; e.g., a decrease in the

https://doi.org/10.1021/acsomega.2c06244
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SLP up to 12, 26, and 52% was documented for dextran, oleic acid, and poly(ethylene glycol) (PEG) treatments, respectively.[76,77,79]

With regard to the *in situ* treatment or synthesis process in an environment containing the coating agents, in most cases, the NPs synthesized in the presence of citrate, dextran, PEG, poly(acrylic acid) (PAA), and hyaluronic acid (HA) show lower SLP values than the uncoated NPs.[80,81] In particular, with the *in situ* PAA coating, a 98% lower SLP was obtained, but this is reasonably attributable to the high decrease in the average diameter of the NPs, from 12 to 5 nm, and the final low value of the saturation magnetization.[81] The reduction in SLP can also be correlated to a decrease in the magnetocrystalline anisotropy and thus in the coercivity as a consequence of the modification of the magnetic order of the surface layers.[80]

Slight improvements in heating efficiency were documented for the *in situ* oleic acid coating of iron oxide NPs with a concentration of 1% v/v due to the enhancement in dispersion in water.[82] Very large increases in the SLP were observed with the *in situ* coating via polyvinylpyrrolidone (PVP) or fucoidan treatments in the order of 60 and 230%, respectively. This was attributed to the role of coating agents in the surface stabilization of NPs, as well as to the growth modifiers acting on the size of NPs, on which the saturation magnetization depends.[81,83]

3.5. Analysis of Nanoparticle Solution Stability. To conclude our experimental studies, we also investigated the stability of the NPs in solution as a crucial parameter for biomedical application development. Figure 6A compares different magnetic suspensions, 6 months after their preparation. In the case of uncoated NPs, we observed their complete precipitation, with sedimentation starting in the first hours after the solution sonication. CMC-coated NPs provided improved stability, even if sedimentation of a part of them can be observed; the use of sodium citrate resulted in the best solution once again, guaranteeing the NP dispersion as well as their long-term storage without precipitation.

Similar outcomes were observed for the NP encapsulation in hydrogels. After 30 min from the magnetic agarose gel preparation, performed according to the procedure described in Section 2.4, we verified the effective formation of the gels (a comparison of the obtained samples is reported in Figure 6B). Also, in this case, the surface coating can play a crucial role in the good dispersion of NPs. While for the uncoated ones, the precipitation of large NP aggregates was observed (possible to be seen by naked eyes at the test tube bottom), sodium citrate gave better dispersion with a homogeneous distribution of NPs, assessed by optical appearance. This behavior opens to further material development, where good dispersion is needed, such as hyperthermia studies in solid environments (to mimic the interaction with biological tissues) or release of molecules (drugs) from thermoresponsive gels.

4. CONCLUSIONS

Fe_3O_4 NPs, with an average size of about 10 nm, were synthesized with the coprecipitation method and then treated with different surface coatings based on sodium citrate or CMC. The three obtained samples (uncoated, citrate-coated, and CMC-coated NPs) were investigated for potential application in magnetic hyperthermia, focusing on heating efficiency and colloidal stability.

We demonstrated that both surface coatings can improve the long-term stability and dispersion of the Fe_3O_4 NPs in solution; moreover, they allow their homogeneous encapsulation in more viscous materials like hydrogels. The best results were obtained with sodium citrate, which is also able to provide a significant enhancement of the heating efficiency, contrarily to CMC. In particular, the improvement in the dispersion of citrate-coated NPs led to the formation of NP aggregates with smaller dimensions, which, in turn, generated a strong enlargement of the AC loop area, which consequently led to an increase in the SLP in the order of 50% compared to the uncoated NPs.

The results obtained from the complete characterization of the Fe_3O_4 NPs in terms of structure, size, aggregation state, colloidal stability, as well as magnetic and heating properties allow for a broad spectrum of comparison with the literature data, providing additional information for the optimal design of magnetic NPs for hyperthermia applications.

Finally, the obtained results showed how the simple NP synthesis approach here employed, i.e., not requiring any pressure control or high boiling solvents, is a step forward toward reproducibility of preparation procedures in standard chemical laboratories and their possible scalability (demonstrated here at the gram scale) and how a simple coating procedure can significantly increase the SLP values.

■ ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge at https://pubs.acs.org/doi/10.1021/acsomega.2c06244.

> XRD pattern of the uncoated Fe_3O_4 NPs with an indication of the characteristic diffraction peaks of Fe_3O_4 and Fe_2O_3 (Figure S1); TEM images of CMC-coated Fe_3O_4 NPs (Figure S2); FTIR spectra of uncoated and coated Fe_3O_4 NPs (Figure S3); magnetization curve and SLP values of an additional batch of uncoated Fe_3O_4 NPs (Figure S4); dynamic hysteresis loops measured on liquid samples containing uncoated and coated Fe_3O_4 NPs performed at different values of the AC magnetic field peak amplitude (Figure S5); time evolutions of the temperature of the magnetic suspensions containing uncoated, citrate-coated, and CMC-coated NPs, following the application of an AC magnetic field with different peak amplitudes (Figure S6); SLP values obtained from thermometric measurements at 100 kHz, varying the peak amplitude of the AC magnetic field (Table S1) (PDF)

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https://doi.org/10.1021/acsomega.2c06244
ACS Omega 2023, 8, 2143−2154

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This manuscript was written through the contribution of all authors. All authors have approved the final version of the manuscript.

Notes

The authors declare no competing financial interest.

■ ACKNOWLEDGMENTS

This work was supported by the Project 18HLT06 RaCHy, which has received funding from the European Metrology Programme for Innovation and Research (EMPIR), cofinanced by the participating states, and from the European Union's Horizon 2020 Programme.

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